

# Nonlinear Modeling of Tumor Growth I: Basic Models

John Lowengrub  
Dept Math, UCI

P. Macklin, Ph.D. 2007 (expected);  
Vittorio Cristini (UCI/UT Health Sci. Center)  
H. Frieboes (UCI)  
S. Wise (UCI)  
X. Zheng (U. Mich.)

# Motivation

- Provide biophysically justified *in silico* virtual system to study
- Help experimental investigations; design new experiments
- Therapy protocols

# Outline

- Introduction to tumor growth

Multiscale complex soft matter problem

- Mathematical Models, Simplifications and Analysis (limited biophysics)

- Numerical Methods

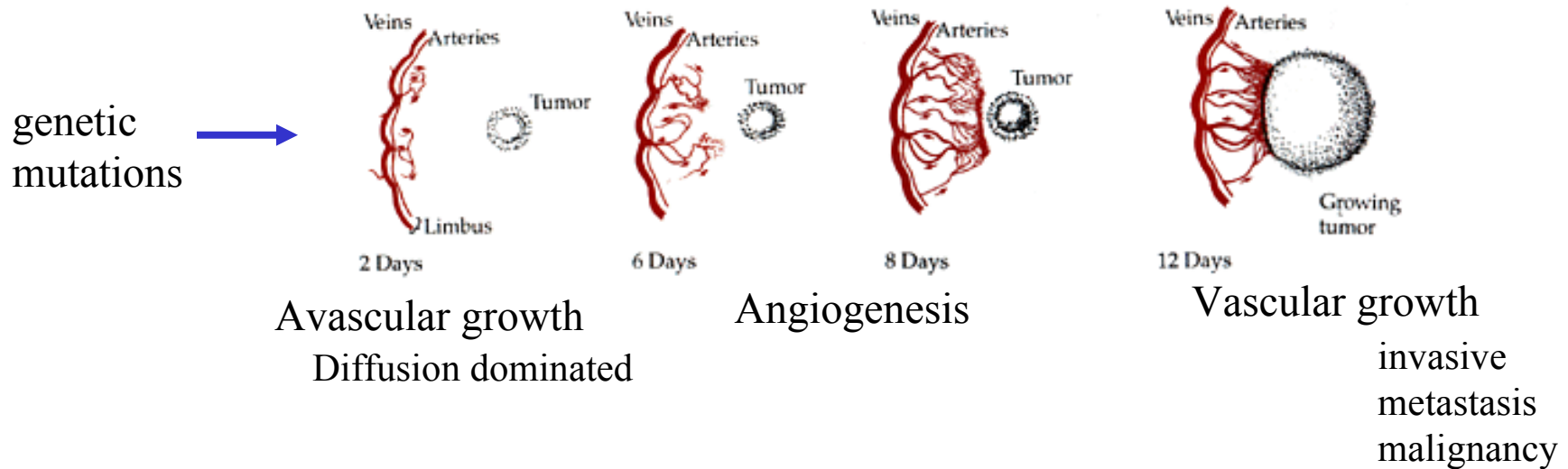
- Results

# The Six Basic Capabilities of Cancer

(Hanahan and Weinberg, 2000)

- Genetic-Level (Nanoscopic)
  - Self-sufficiency in Growth Signals
  - Insensitivity to Growth-inhibitory Signals
  - Evasion of Programmed Cell Death
  - Limitless Replicative Potential
- Tissue-Level (Microscopic)
  - Tissue Invasion and Metastasis
  - Sustained Angiogenesis

# Example of solid tumor growth

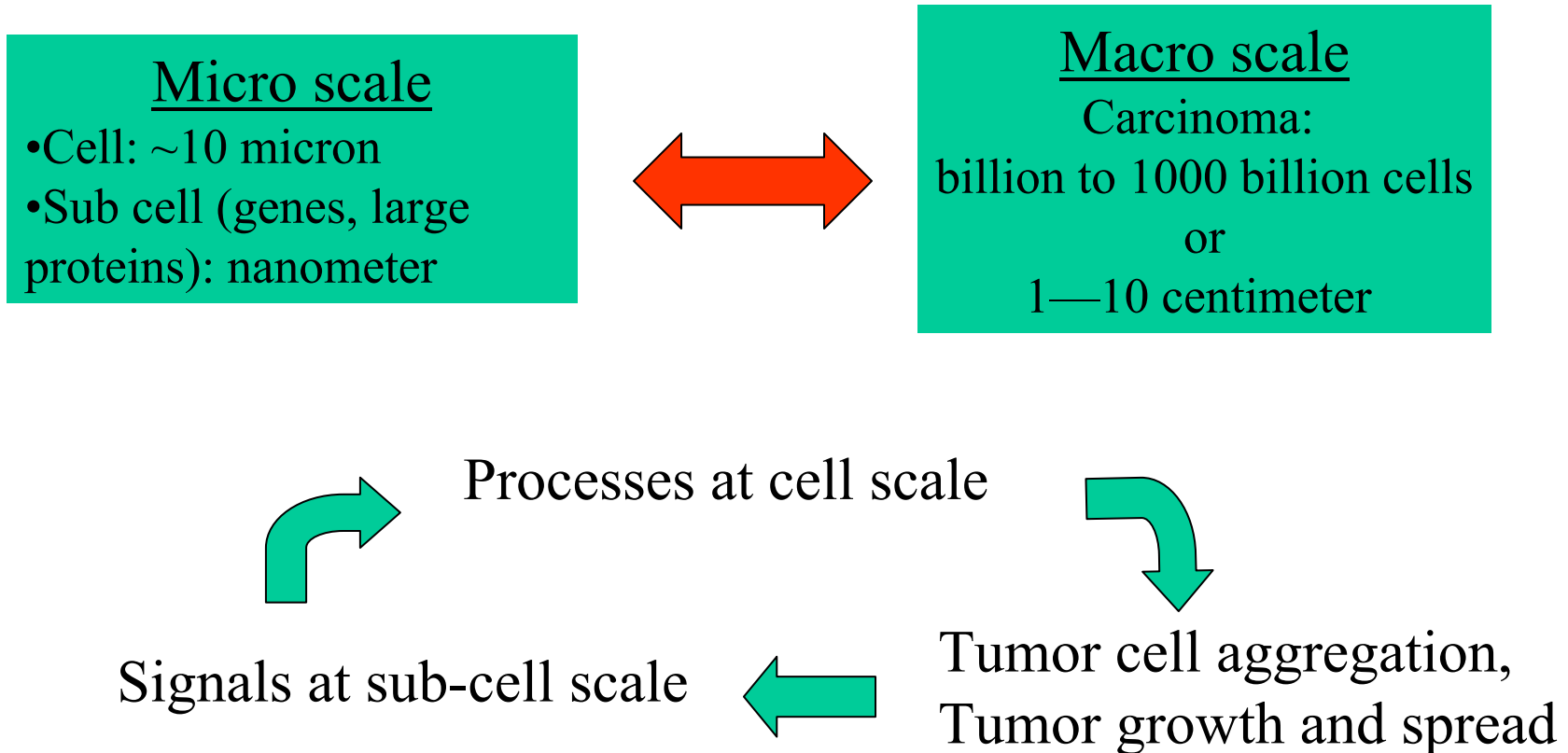


- Goal: Model all Phases of growth

In this talk, I will simplify the biophysics.  
More complex biophysics will be considered  
in subsequent talks.

# Cancer/Solid Tumor

- complex micro-structured soft matter

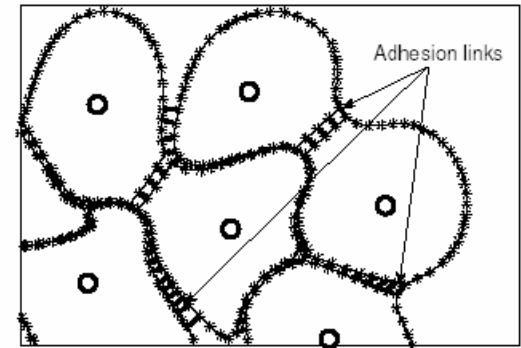
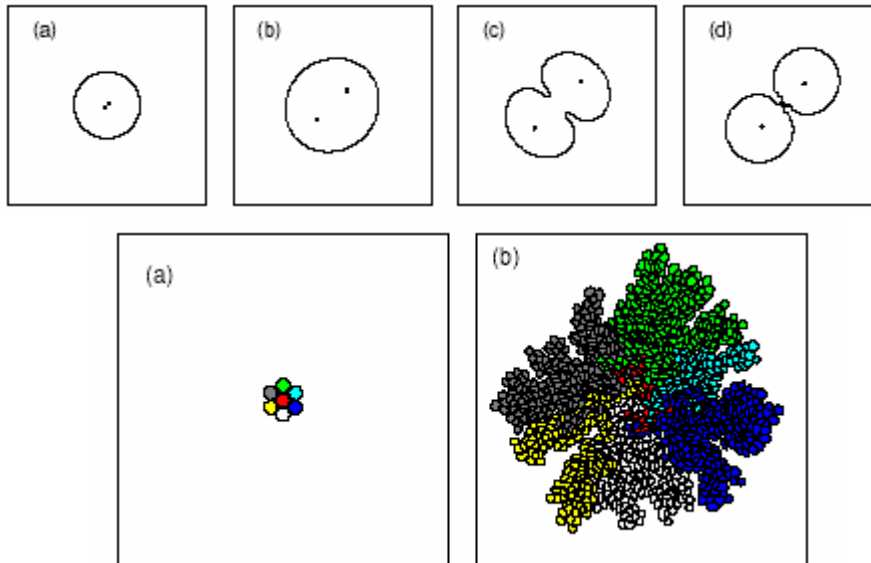


# Modeling Choices

## Discrete models:

### Single-cell models:

Rejniak, Math Biosci. Eng, 2004



- Immersed boundary method.
- Direct account for cell-cell adhesive links/mitosis
- Limited to small numbers of cells (um scale)

# Modeling Choices Contd

Q-Potts:

- 3D Cell described by 27 lattice sites

- Total energy:

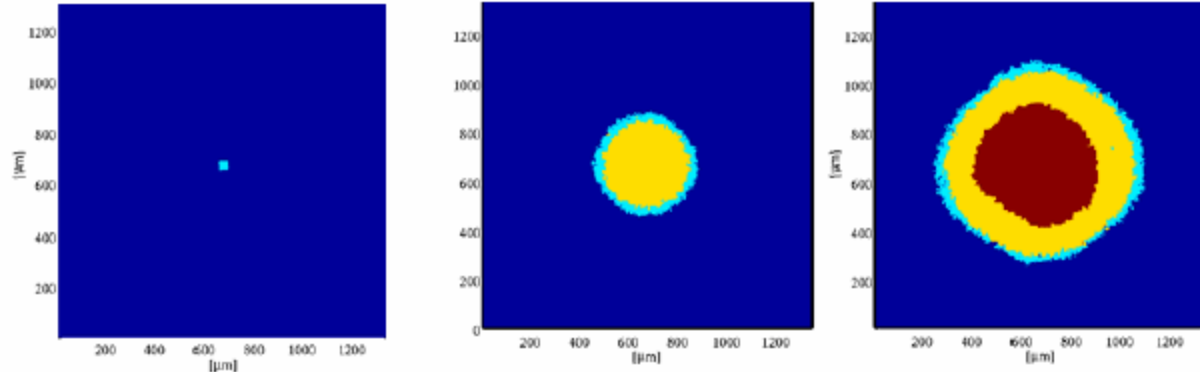
$$H = \sum_{\text{lattice sites}} J_{\tau(S_1)\tau(S_2)} [1 - \delta(S_1, S_2)] + \sum_{\text{cells}} \gamma \cdot (v - V^T)^2.$$

- Monte Carlo:

$$P = \begin{cases} 1, & \Delta H < 0 \\ e^{-\frac{\Delta H}{k_b T}}, & \Delta H \geq 0 \end{cases},$$

- Direct account of cell-volume and adhesion forces
- Limited to small numbers of cells (um scale)

Jiang et al, Biophys. J. (2005)





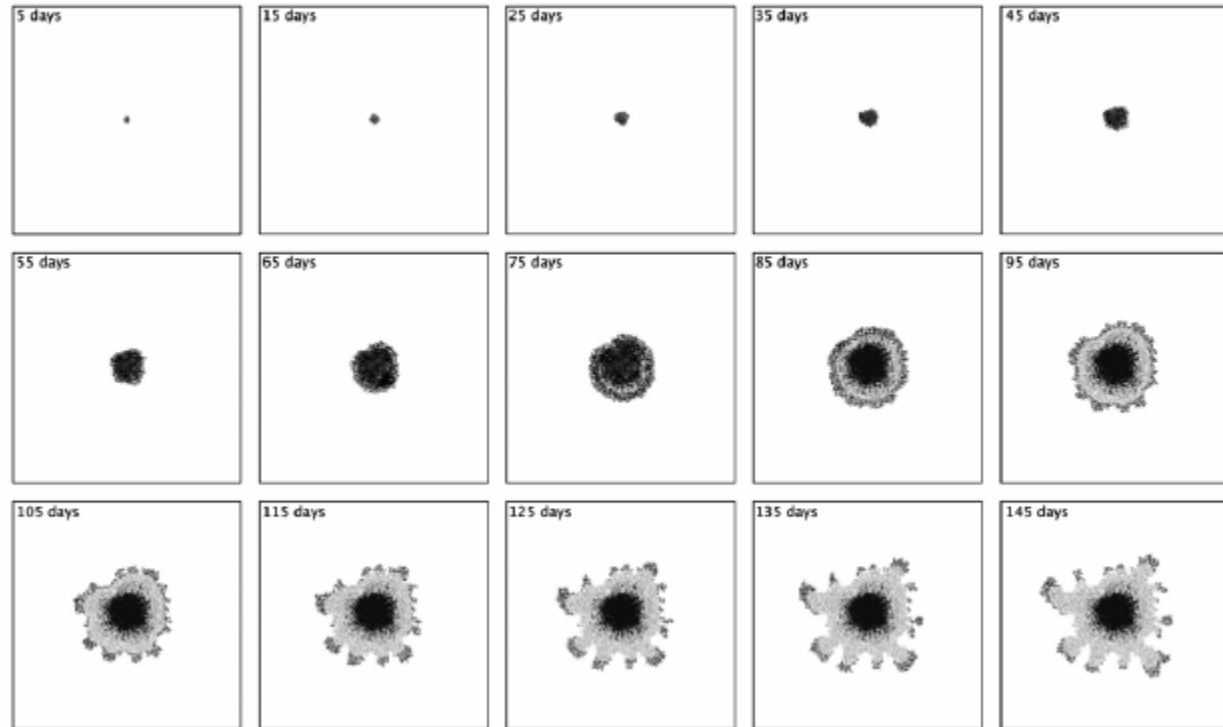
# Modeling Choices Contd

Anderson, Math. Med. Biol, 2005

## Cellular automata

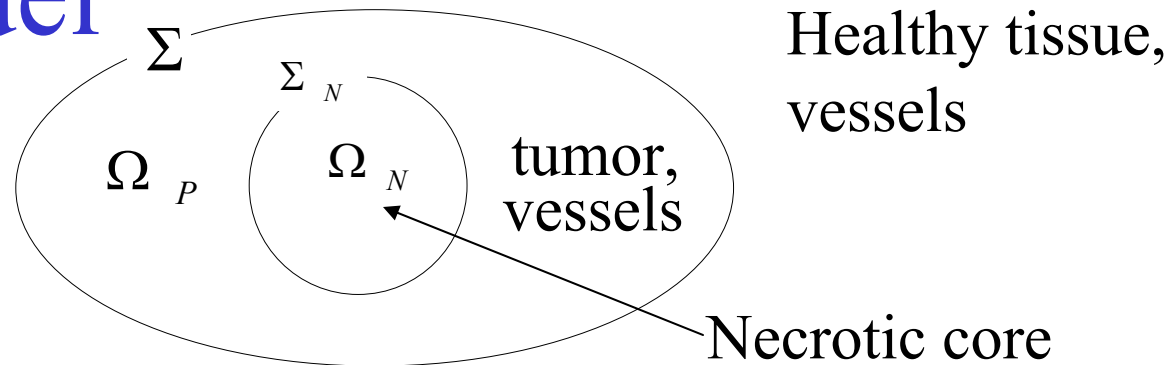
- Cells occupy lattice sites
- Motion according to

$$n_{i,j}^{q+1} = n_{i,j}^q P_0 + n_{i+1,j}^q P_1 + n_{i-1,j}^q P_2 + n_{i,j+1}^q P_3 + n_{i,j-1}^q P_4.$$



- Account for adhesion/proliferation
- Does not track cell size or shape
- Somewhat larger scale  $\sim 1\text{mm}$
- To get to larger (cm) scale need continuum model

# Present model



- Continuum approximation: super-cell macro scale    cm scale
- Role of **cell adhesion and motility** on tissue invasion and metastasis  
Idealized mechanical response of tissues
- **Coupling between growth and angiogenesis** (neo-vascularization):  
necessary for maintaining uncontrolled cell proliferation
- **Genetic mutations**: random changes in microphysical parameters cell  
apoptosis and adhesion
- **Limitations**: poor feedback from macro scale to micro scale  
(Greenspan, Byrne & Chaplain, Anderson & Chaplain, Levine...)

# Cell proliferation and tissue invasion

Greenspan, Chaplain, Byrne, ...

Assume constant tumor cell density:  
cell velocity

Assume 1 diffusing nutrient of concentration  $\sigma$

Cell proliferation: in the tumor is a balance of mitosis and apoptosis (mitosis is responsible for reproduction of mutated genes) and is one of the two main factors responsible for tissue invasion

Cell-to-cell adhesion

$$\nabla \cdot \mathbf{u} = \begin{cases} \lambda_M(\sigma) - \lambda_A & \text{in } \Omega_P \\ -\lambda_N & \text{in } \Omega_N = \{\mathbf{x} \mid \sigma(\mathbf{x}, t) \leq \sigma_N\} \end{cases}$$

$$P = \tau \kappa \text{ on } \Sigma$$

Viability concentration

Darcy's law

$$\mathbf{u} = -\mu \nabla P$$

Rate of enzymatic breakdown of necrotic cells (death due to lack of nutrient)



Cell mobility: reflect strength of cell adhesion to other cells and to the Extra-Cellular Matrix (ECM), the other main factor leading to tissue invasion

Spatial distribution of the oncotic pressure



Cell death responsible for release of angiogenic factors: INPUT TO ANGIOGENESIS

# Evolution of nutrient: Oxygen/Glucose

Greenspan, Chaplain, Byrne, ...

=0 (quasi-steady assumption). Tumor growth time scale (~1 day) large compared to typical diffusion time (~1 min)

$$\frac{\partial \sigma}{\partial t} = \nabla \cdot (D \nabla \sigma) - \lambda_C \cdot \sigma + \lambda_B (\sigma_B - \sigma, P_B - P, \mathbf{x}, t)$$

Diffusion

nutrient concentration in blood


Oncotic pressure: affects blood flow and delivery of nutrients (and chemotherapy drugs)

Nutrient consumption by the cells

Blood-to-tissue nutrient transfer rate function. Spatial distribution of capillaries: **OUTPUT FROM ANGIOGENESIS**

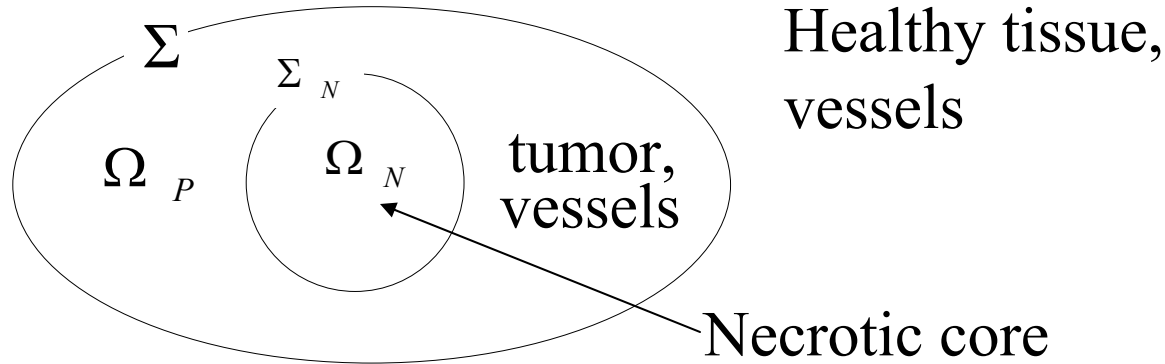
# Limited Biophysics

- Simplified cell-cycling model  $\lambda_M(\sigma) = b\sigma$
- Simplified Blood-tissue transfer  $\lambda_B(\sigma_B - \sigma, P_B - P, \mathbf{x}, t) = \lambda_B \cdot (\sigma_B - \sigma)$
- Avascular or fully vascularized growth (i.e. no angiogenesis)

- 
- Insight to biophysical system
  - Benchmark for more complicated systems

# Basic model

Greenspan, Chaplain, Byrne, Friedman-Reitich, Cristini-Lowengrub-Nie,...



## Nutrient

$$0 = D\nabla^2\sigma + \Gamma,$$

$$\Gamma = -\lambda_B (\sigma - \sigma_B) - \lambda \sigma.$$

$$(\sigma)_\Sigma = \sigma^\infty$$

## Pressure

$$\mathbf{u} = -\mu\nabla P, \quad \nabla \bullet \mathbf{u} = \begin{cases} \lambda_P & \text{in } \Omega_P \\ -\lambda_N & \text{in } \Omega_N \end{cases}$$

$$(P)_\Sigma = \gamma\kappa \quad \lambda_P = b\sigma - \lambda_A,$$

$$V = -\mu \mathbf{n} \cdot (\nabla P)_\Sigma.$$

normal velocity

# Nondimensionalization

(Cristini, Lowengrub and Nie, J. Math. Biol. 46, 191-224, 2003)

Intrinsic length scale:  $L_D = D^{\frac{1}{2}} (\lambda_B + \lambda)^{-\frac{1}{2}}$

Adhesion time scale:  $\lambda_R^{-1}$ ,  $\lambda_R = \gamma\mu / L_D^3$

## Nondimensional Parameters:

•Vascularization:  $B = \frac{\sigma_B}{\sigma^\infty} \frac{\lambda_B}{\lambda_B + \lambda}$

•Apoptosis vs. mitosis  $A = \frac{\lambda_A/\lambda_M - B}{1 - B}$  healthy tissue:  $A \approx 1$   
genetic mutation:  $A < 1$

•Mitosis vs. adhesion  $G = \frac{\lambda_M}{\lambda_R} (1 - B)$   $\lambda_M = b\sigma^\infty$

Mitosis rate

•Necrosis vs. mitosis  $G_N = \lambda_N / \lambda_M$

•Viability  $N = \frac{\sigma_N}{\sigma_\infty} - B$

# Nondimensional basic system

nutrient

$$c = (\sigma / \sigma_\infty - B) / (1 - B)$$

pressure

$$p = P / (\gamma / L_D)$$

Free Boundary Problem:

$$\Delta c = c \quad \text{in } \Omega_P \quad \Delta p = G \cdot \begin{cases} (A - c) & \text{in } \Omega_P \\ G_N & \text{in } \Omega_N \end{cases}$$

where  $\Omega_N(t) = \{ \mathbf{x} \mid c(\mathbf{x}, t) \leq N \}$

On  $\Sigma$  :

$$p = \kappa$$

$$c = 1$$

$$\mathbf{n} \cdot \frac{d\mathbf{x}_\Sigma}{dt} = V = -\nabla p \cdot \mathbf{n}$$



# Evolution of a spherical tumor:

1. Low vascularization:

$$A > 0 \quad \text{and} \quad G > 0$$

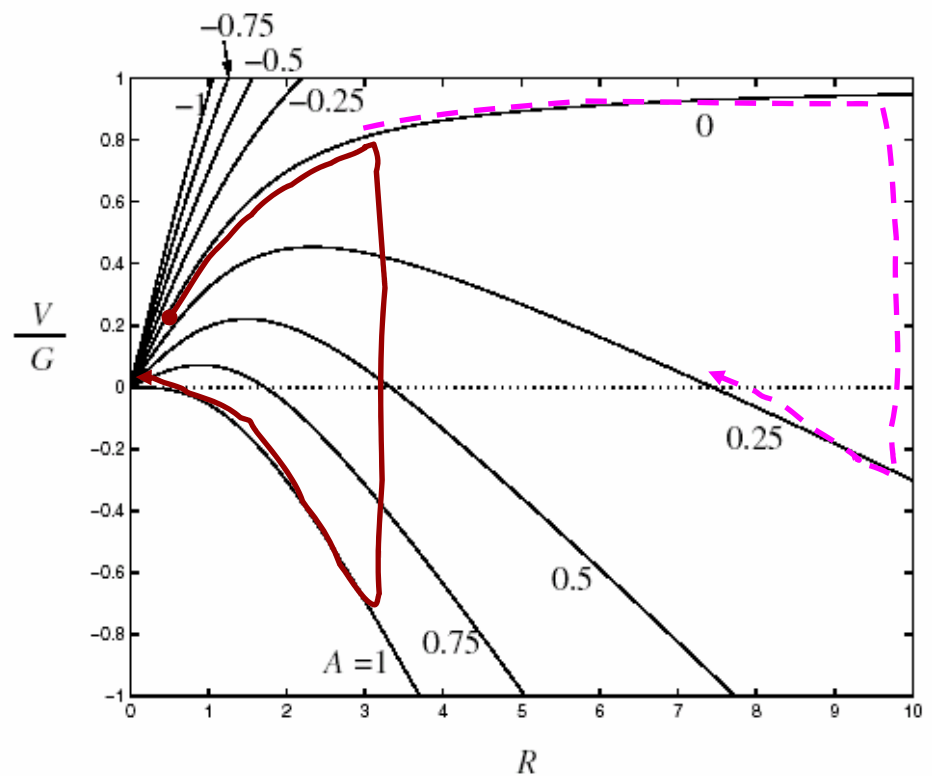
Dormant state, Shrinkage to zero

2. Moderate vascularization:  $A < 0$  and  $G > 0$

Mimic angiogenesis, unbounded growth

3. High vascularization:  $G < 0$

Unbounded growth, shrinkage to zero



Agreement w/ observed growth

Treatment

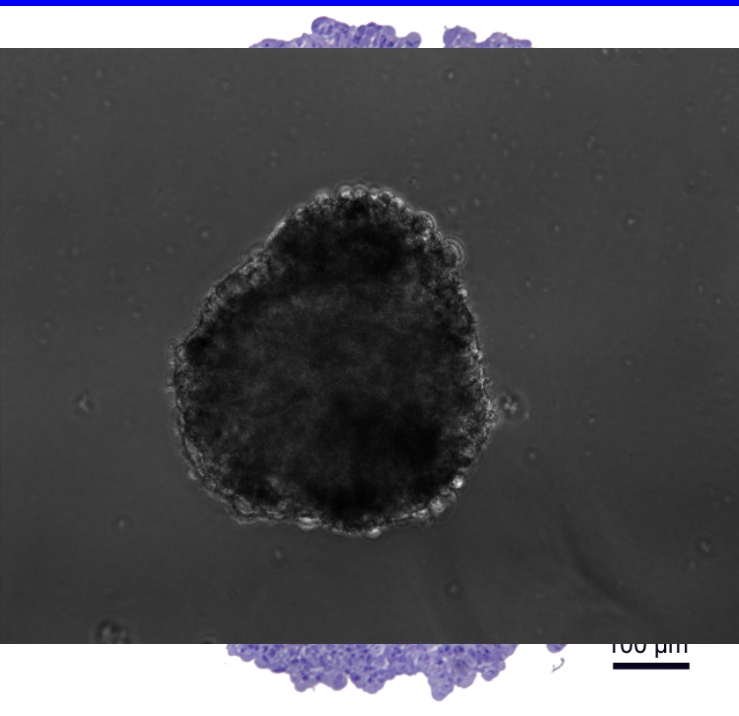


Transition  
between  
phases

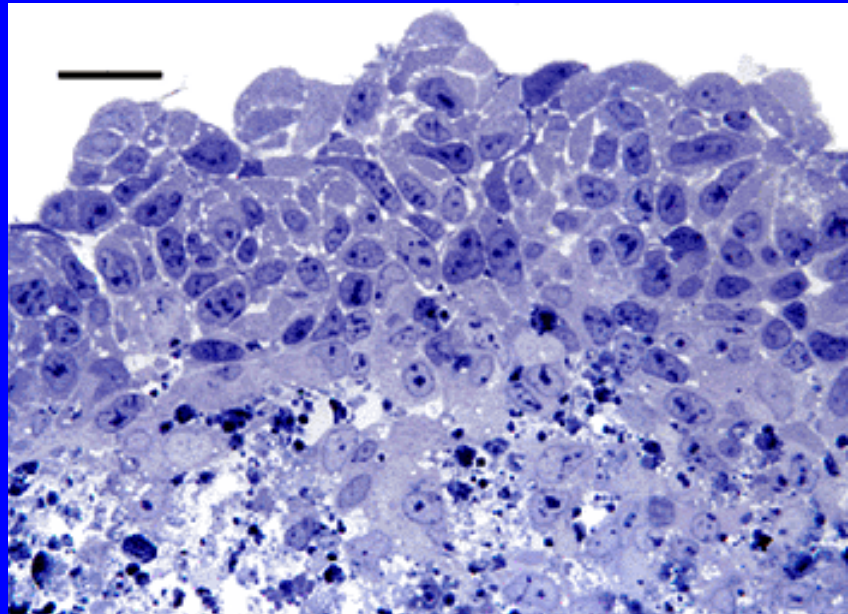
# Tumor Spheroids: *In vitro* study

In vitro growth: No vascularization (diffusion-dominated)

Dormant (steady) states



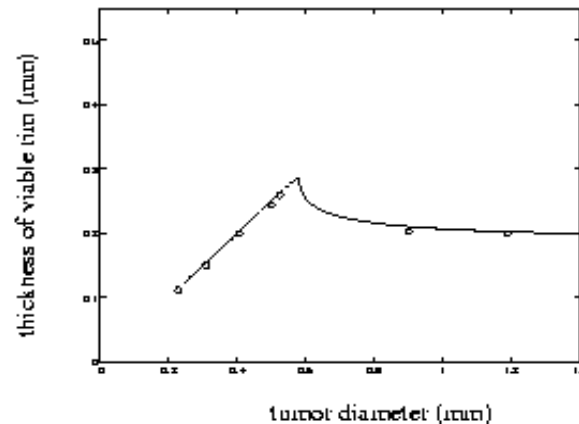
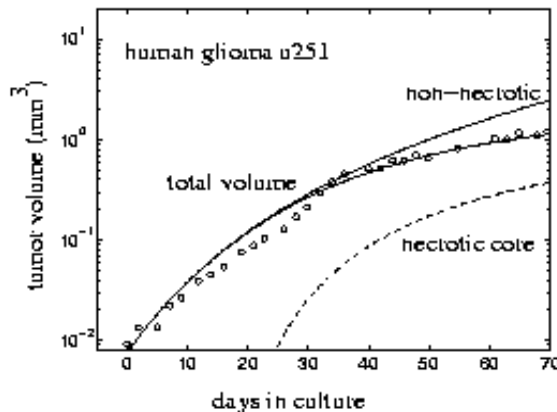
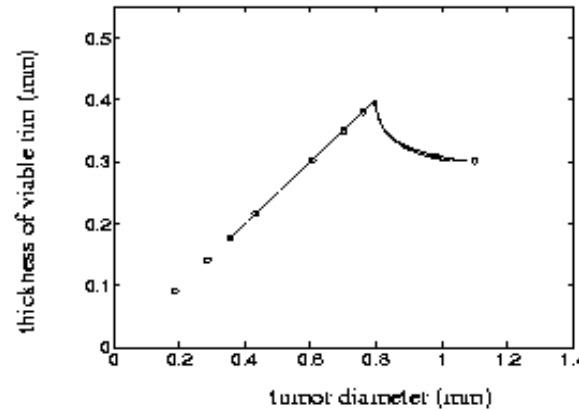
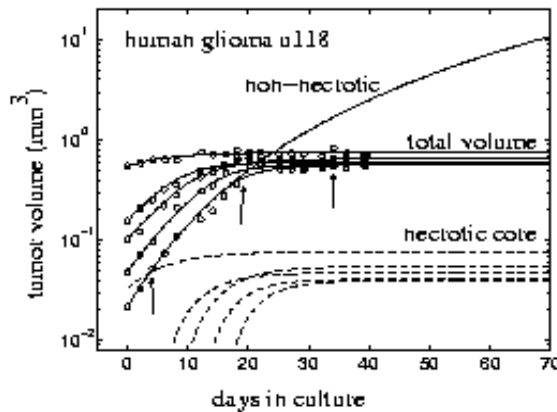
One micron section of tumor spheroid showing outer living shell of growing cells and inner core of necrosis.



3-D video holography through biological tissue  
P. Yu, G. Mustata, and [D. D. Nolte](#), Dept. of  
Physics, Purdue University

# Tumor Modeling: The basic model

## Model validation:



In vitro data:  
Karim & Carlsson  
Cancer Res.



- Agreement w/ observed growth
- Determine microphysical parameters

# Microphysical parameters

- $A=0$ ,  $G_N = \begin{cases} 4.0 & u118 \\ 0.31 & u251 \end{cases} \quad N \approx 10^{-2}$

$$\lambda_M \approx 0.3 \text{ day}^{-1}$$

$$D \approx 3 \times 10^{-3} \text{ mm}^2 / s$$

$$\lambda_C \approx 2 \text{ s}^{-1}$$

$$L \approx 4 \times 10^{-2} \text{ mm}$$

(approximately 7 cells)

$G$  can be estimated indirectly.

# Estimation of $G$

Frieboes, Cristini, et al. Clin. Canc. Res., 2006.

Low vascularization regime.  $B=0$ ,  $G>0$ .

In proliferating region,

At tumor boundary,

$$P \sim L_D^2 \lambda_M / \mu$$

$$P \sim \tau / L_D R$$

$R$  – nondimensional tumor radius

At steady-state,

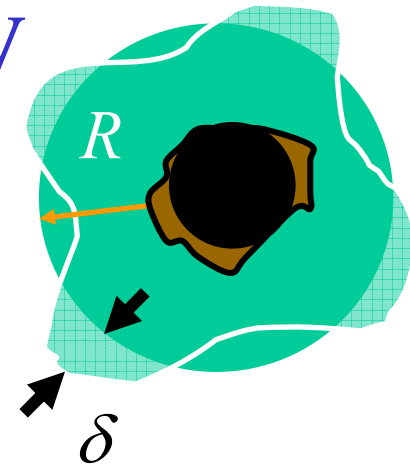
$$L_D^2 \lambda_M / \mu \sim \tau / L_D R \quad \text{which implies} \quad G \sim 1 / R$$

  $G \sim 0.1$  for u118 and u251 (N=0, A>0)

(underestimate)

{ Experiments  
Linear stability theory } needed for further refinement.

# Morphological stability



Perturbation

$$r_{\Sigma} = R(t) + \delta(t) \begin{cases} \cos(l\theta) & \text{in } 2D \\ Y_{lm}(\theta, \phi) & \text{in } 3D \end{cases}$$

Underlying Growth  
 $d=2,3$

$$G^{-1} \frac{dR}{dt} = -\frac{AR}{d} + \begin{cases} I_1(R)/I_0(R) & \text{in } 2D \\ \coth(R) - 1/R & \text{in } 3D \end{cases} + F(N, G_N, R)$$

→  $G_N = G_N^{steady}(R, N, A)$  such that  $dR/dt = 0$   
(balance between proliferation, necrosis and apoptosis)

If  $N=0$ , then reduces to  $A = A^{steady}(R)$

Shape evolution

$$\left(\frac{\delta}{R}\right)^{-1} \frac{d}{dt} \left(\frac{\delta}{R}\right) = H_{growth}(l, R, A, G, G_N, N) - H_{decay}(l, R, A, G, G_N, N)$$

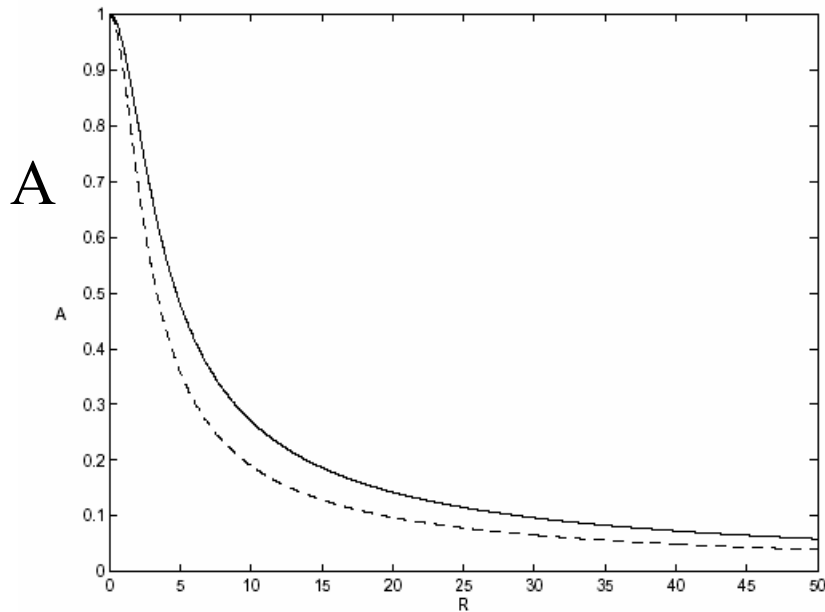
Self-similar evolution

→  $G = G^{crit}(l, R, G_N, N, A)$  such that  $d(\delta/R)/dt = 0$

If  $N=0$ , then can also get  $A = A^{crit}(l, R, G)$

# Nontrivial steady states

$$\dot{R} = 0 \quad \text{and} \quad \dot{\delta} = 0 \quad \xrightarrow{\text{Non-necrotic.}} \quad \begin{aligned} A &= A^{\text{steady}}(R) \\ G &= G^{\text{crit}}(l, R, A^{\text{steady}}) \end{aligned}$$

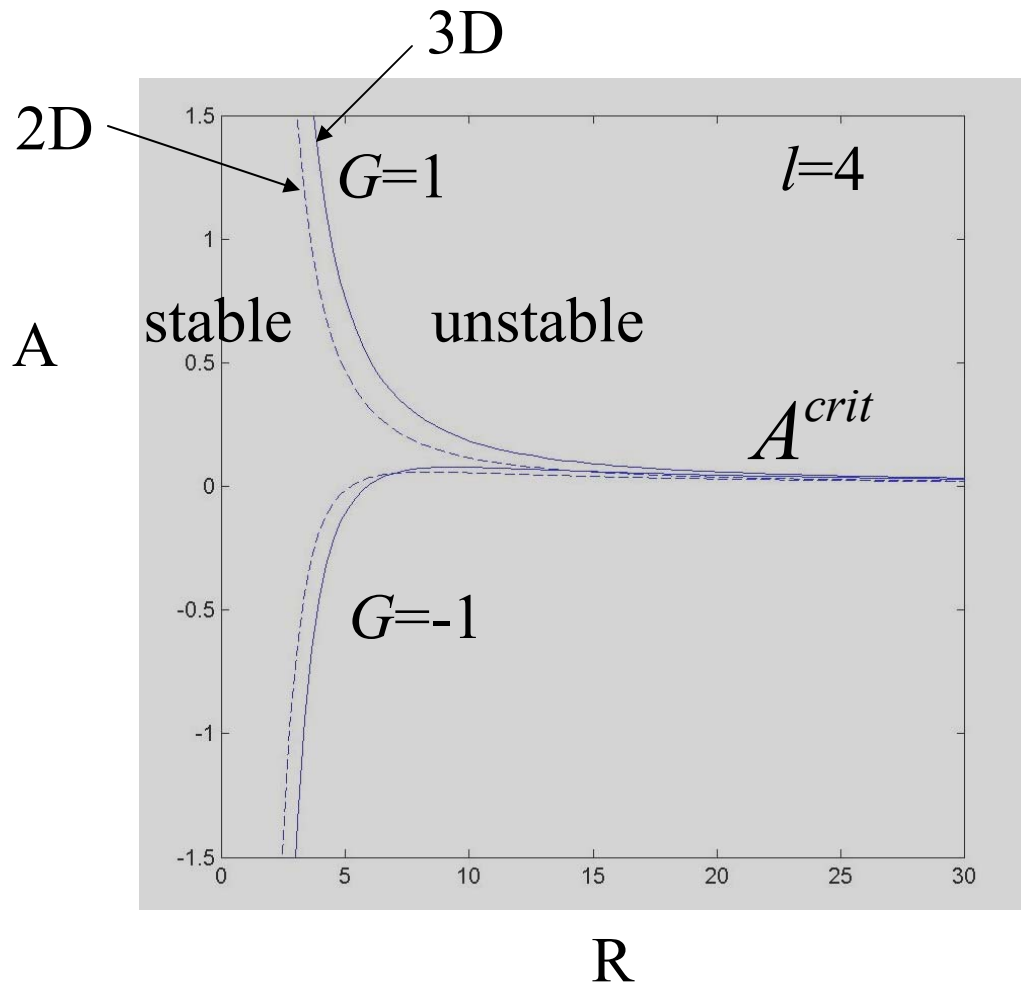


$R_\infty$  (steady radius)

$$G_l = \begin{cases} \frac{1}{R_\infty^3} \frac{2l(l^2-1)}{2-A \left[ 2+R_\infty \frac{I_{l+1}(R_\infty)}{I_l(R_\infty)} \right]} & d = 2 \\ \frac{1}{R_\infty^3} \frac{3l(l-1)(l+2)}{3-A \left[ 3+R_\infty \frac{I_{l+\frac{3}{2}}(R_\infty)}{I_{l+\frac{1}{2}}(R_\infty)} \right]} & d = 3 \end{cases}$$

# Self-similar evolution

$$\left(\frac{\delta}{R}\right)' = 0 \quad \xrightarrow{\text{Non-necrotic.}} \quad A = A^{crit}(l, R, G)$$



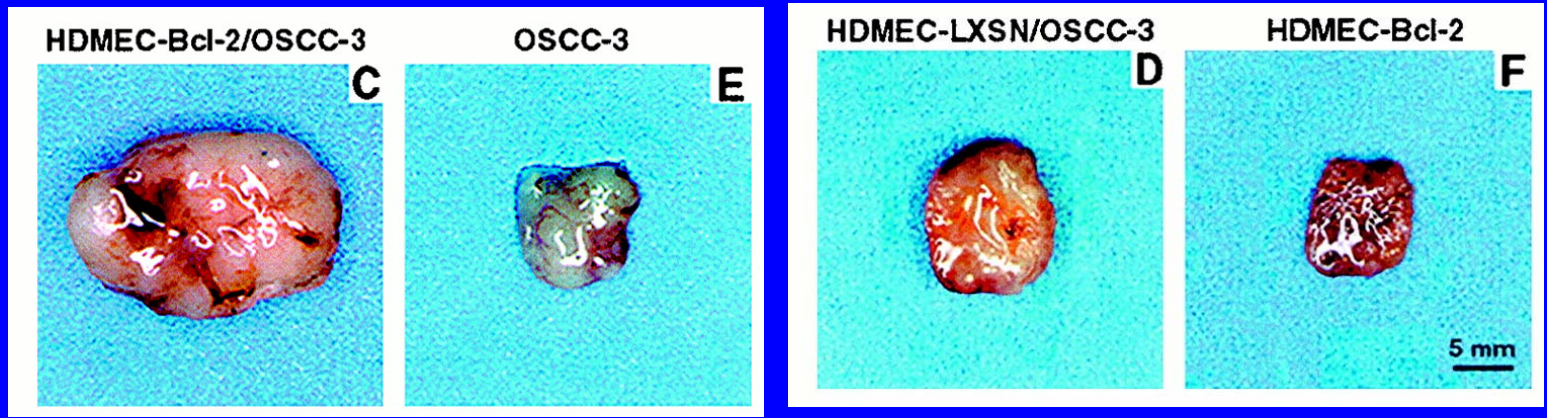


# Summary of Linear Stability Results

- Qualitatively similar for 2D/3D
- Necrosis enhances instability

1. Low vascularization ( $A, G > 0$ ) (diffusion-dominated):
  2. Moderate vascularization: ( $A < 0, G > 0$ )
  3. High vascularization: ( $G < 0$ )
- Stable/Shape-preserving/Unstable
- Stable

Experimental evidence  
(Polverini et al.,  
Cancer Res. 2001)



Shape instability with high vascularization



Vascular/mechanical inhomogeneity

# Nonlinear Simulations

Non-necrotic.

## Boundary integral methods

2D: Cristini, Lowengrub and Nie, J. Math. Biol. 46, 191-224, 2003

3D: Li, Lowengrub, Pham, Cristini, Nie. In preparation

Modified pressure:

$$\tilde{p} = p + G(c-1) - AG |\mathbf{x}|^2 / 2d \quad \text{then} \quad \Delta \tilde{p} = 0$$

2D: Double-layer potentials for  $\tilde{p}$  and  $c$ :

$$c(\mathbf{x}) = \frac{1}{2\pi} \int_{\Sigma} \beta(\mathbf{x}') \mathbf{n} \cdot \nabla K_0(|\mathbf{x} - \mathbf{x}'|) d\Sigma(\mathbf{x}')$$

$$\tilde{p}(\mathbf{x}) = \int_{\Sigma} \mu(\mathbf{x}') \mathbf{n} \cdot \nabla G(\mathbf{x} - \mathbf{x}') d\Sigma(\mathbf{x}')$$

$K_0(r)$

Modified Bessel function

$$G(\mathbf{x}) = \frac{1}{2\pi} \log |\mathbf{x}|$$

Green's function

2<sup>nd</sup> kind Fredholm integral equations for  $\beta, \mu$

$V$  (normal velocity) evaluated by the Dirichlet-Neumann Map

# Difficulties

- Singular kernels

- Compute singular contribution explicitly to remove singularity.
- Spectrally accurate discretization.

• Stiffness  $V \sim H(\kappa_s)$    $\Delta t \leq \Delta s^3$   
Explicit methods.

2D: Equal arclength parametrization.

Special choice of tangential velocity.

Small scale decomposition.

Nonstiff, explicit time integration schemes

# Numerical Results

- Steady-states
- Self-similar evolution
- Stable evolution
- Diffusional Instability

# Nonlinear Steady-States

Friedman, Reitich 2001

$$\dot{R} = 0 \quad \text{and} \quad \dot{\delta} = 0$$

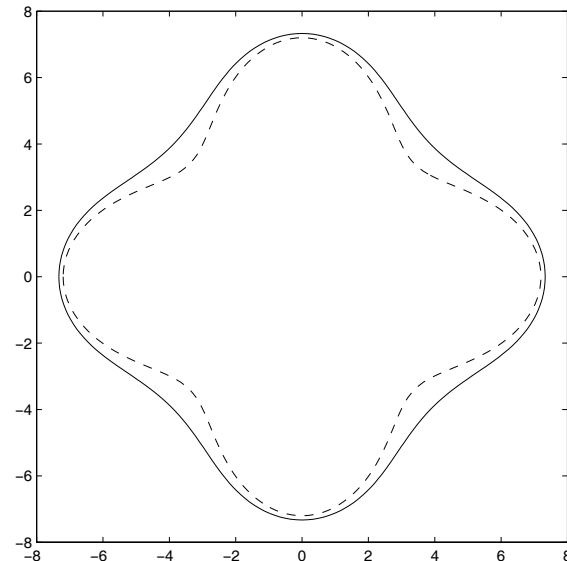
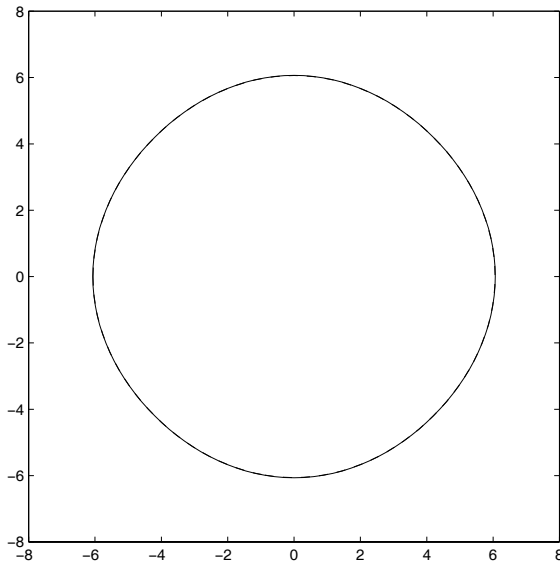


$$A = A^{steady}(R)$$
$$G = G^{crit, Nonlinear}(l, R, A^{steady})$$

$\delta/R=0.01$

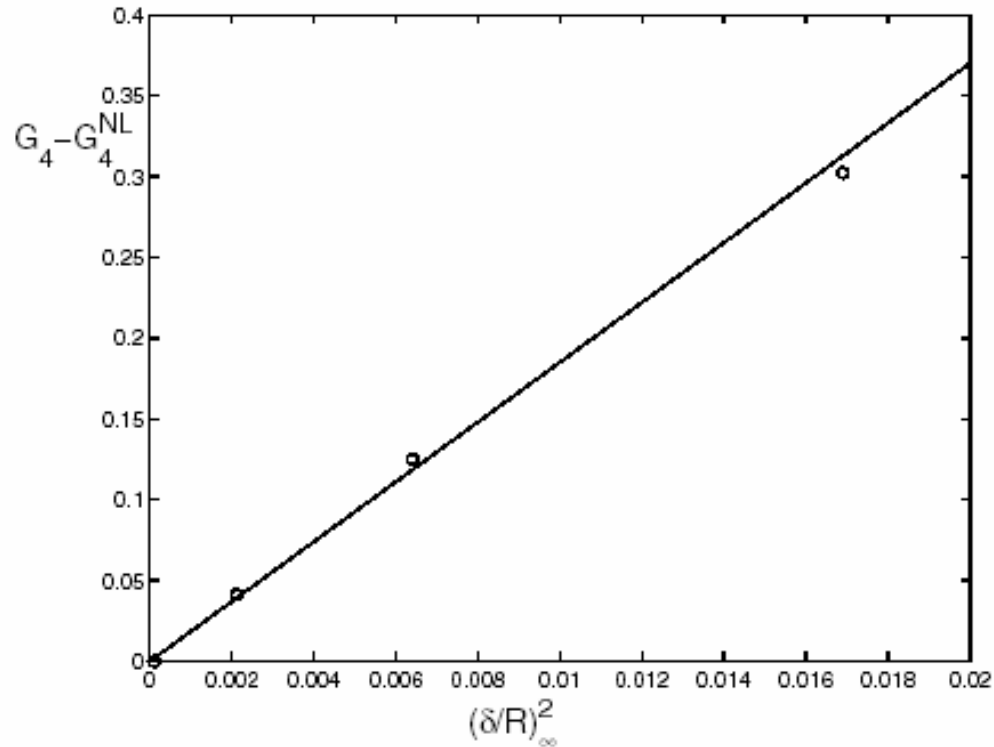
$l=4, A=0.3$

$\delta/R=0.20$



Dashed: linear solution, Solid: Nonlinear solution

# Critical G for nontrivial steady state

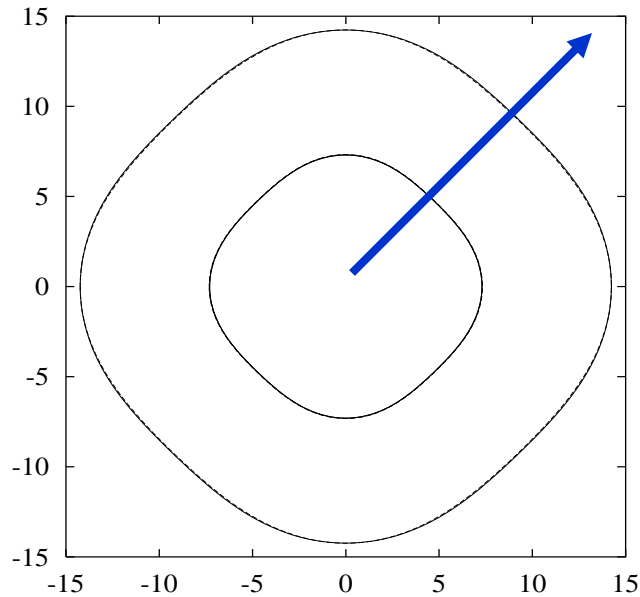


- Convergence to linear theory for small perturbations
- Nonlinearity reduces the critical G

# Examples of Shape preserving evolution

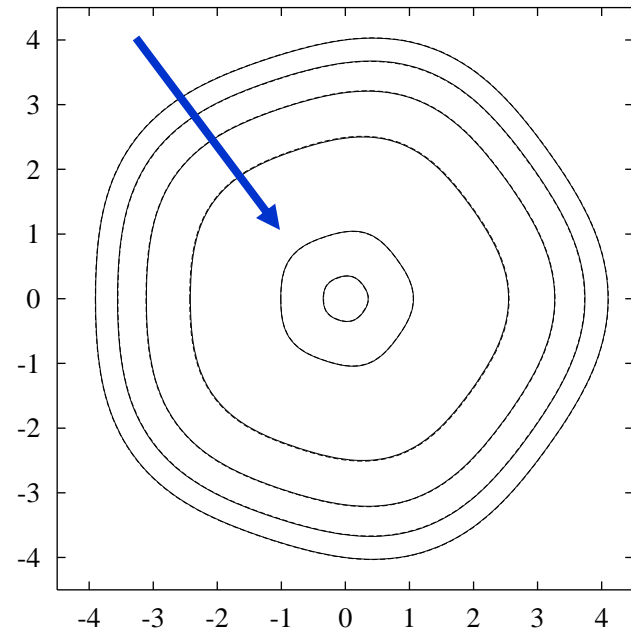
$$A = A^{crit}(l, R, G)$$

Growth



$l=4, G=1$

Shrinkage



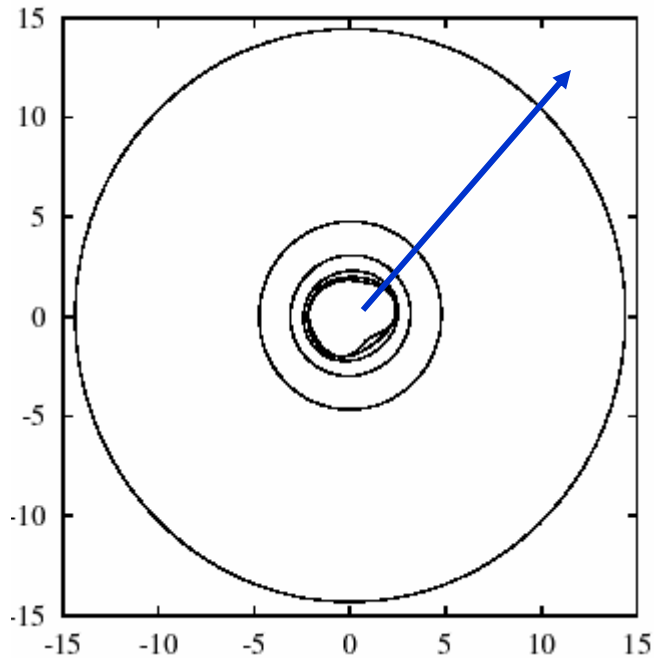
$l=5, G=1$

- Strongly suggests existence of nonlinear self-similar evolution

# Stable evolution

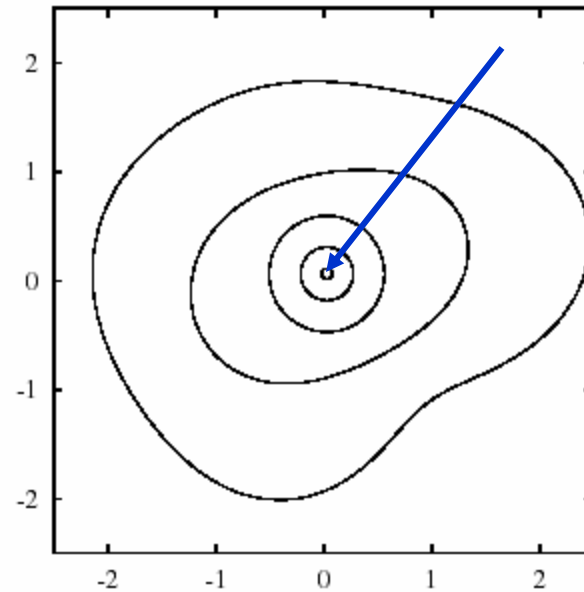
Highly vascularized regime.

Growth



$$A=0.8, G=-5$$

Shrinkage



$$A=0.2, G=-5$$

- Nonlinear results consistent with linear theory.



# Diffusional Instability

2D: Cristini, Lowengrub and Nie, J. Math. Biol. 46, 191-224, 2003

3D: Li, Lowengrub, Pham Cristini, and Nie. In preparation

$$A=0.6, G=20$$

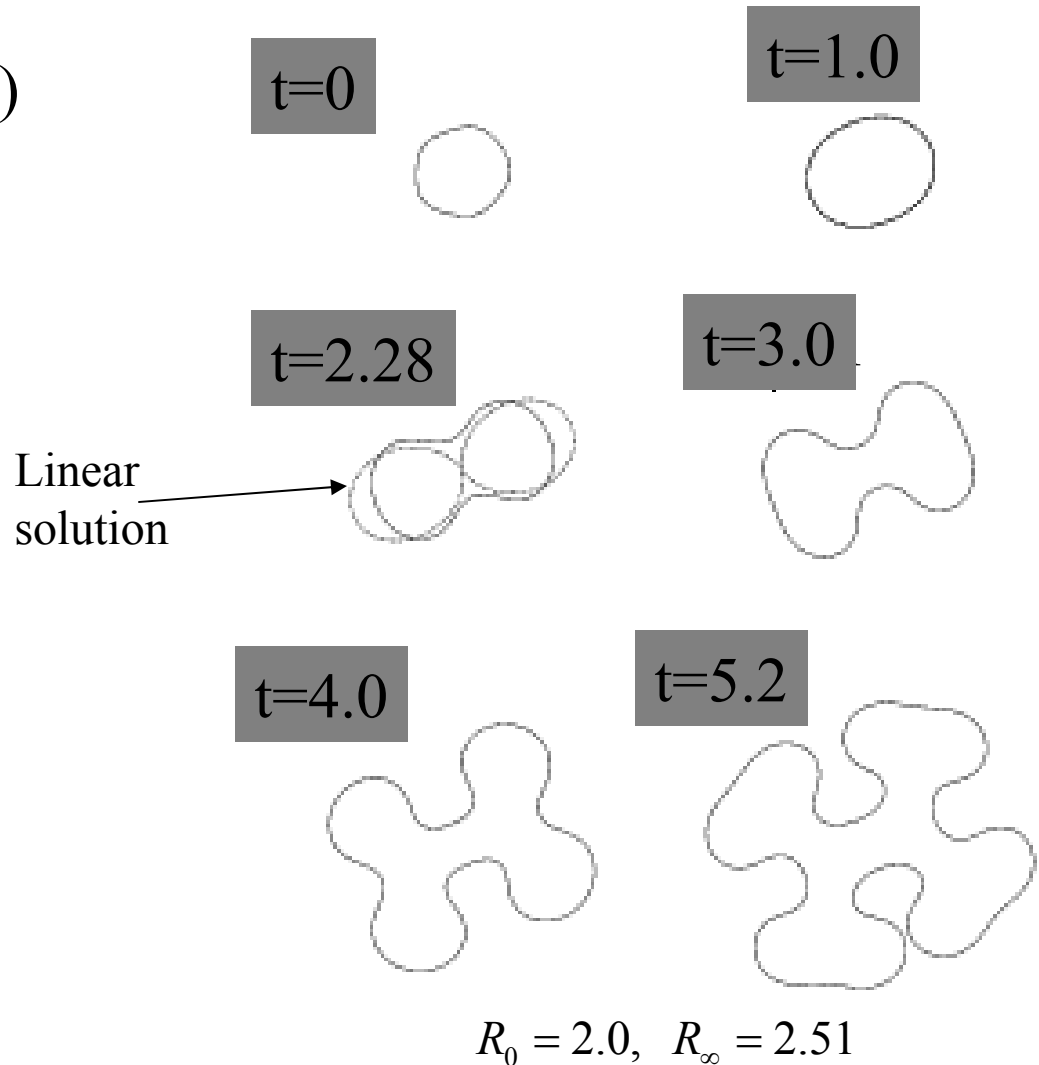
**Avascular** (tumor spheroid)  
(low cell-to-cell adhesion)

$$G > G_{critical}$$

- **Growth-by-budding**  
ejection of cells from bulk

- **Topology change**  
Capture of healthy tissue.

- **Deviation from linear theory**

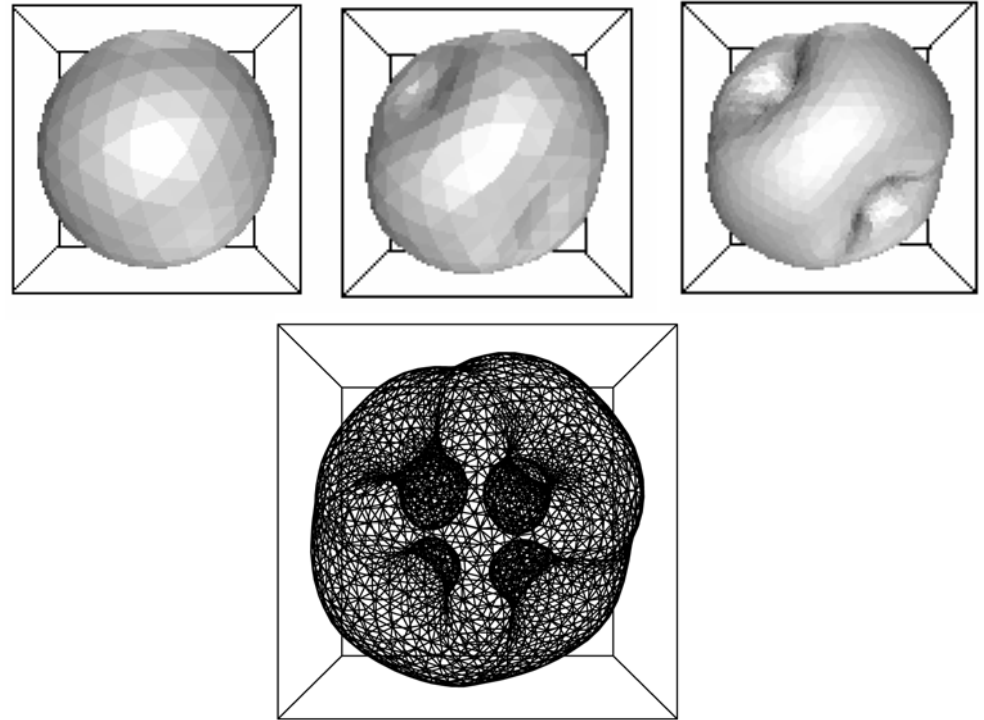


# 3D Evolution Similar

3D:, Li, Cristini, Nie, Lowengrub. DCDS-B, in press.

**Avascular** (tumor spheroid)  
(low cell-to-cell adhesion)

$$G > G_{critical}$$



Numerical method:

- Single layer representation of c.
- Vector potential representation for  $\tilde{p}$

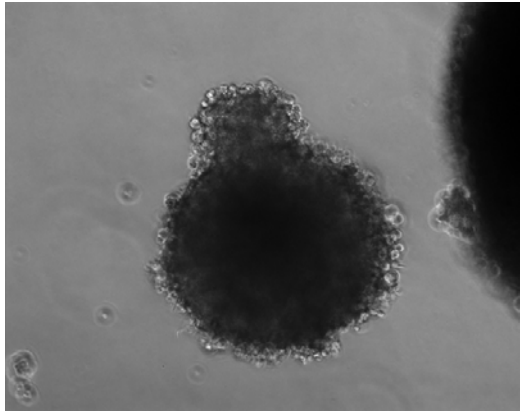
$$p(\mathbf{x}) = \frac{1}{4\pi} \int_{\Sigma} \nu(\mathbf{x}') \frac{(\mathbf{x}' - \mathbf{x}) \cdot \mathbf{n}(\mathbf{x})}{|\mathbf{x}' - \mathbf{x}|^3} dS(\mathbf{x}')$$

- Adaptive surface mesh  
Cristini et al. J. Comp. Phys, 2001

- Rescaled coordinates
- Adaptive quadrature of singular integrals
- Smoothing

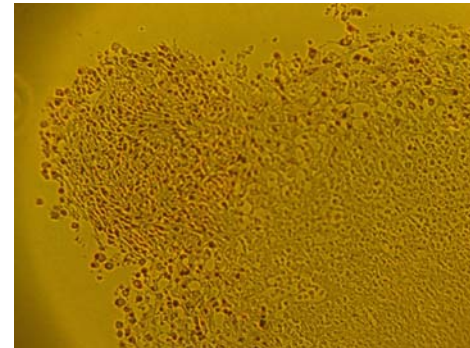
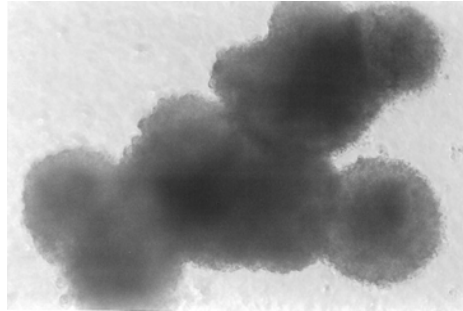
# Experimental Evidence

- Diffusional Instability. (Tumor spheroids)

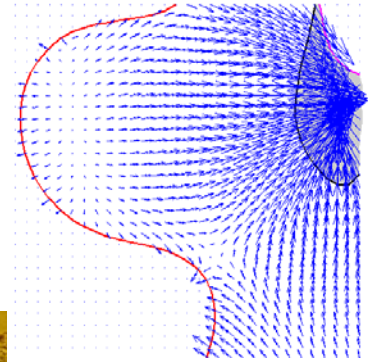


Frieboes, *et al.*

glioblastoma



Swirling ejection from bulk



Velocity field  
(simulation)

- Theory:

Possible mechanism for invasion into soft tissue

Cristini, Lowengrub, Nie *J. Math. Biol* (2003)

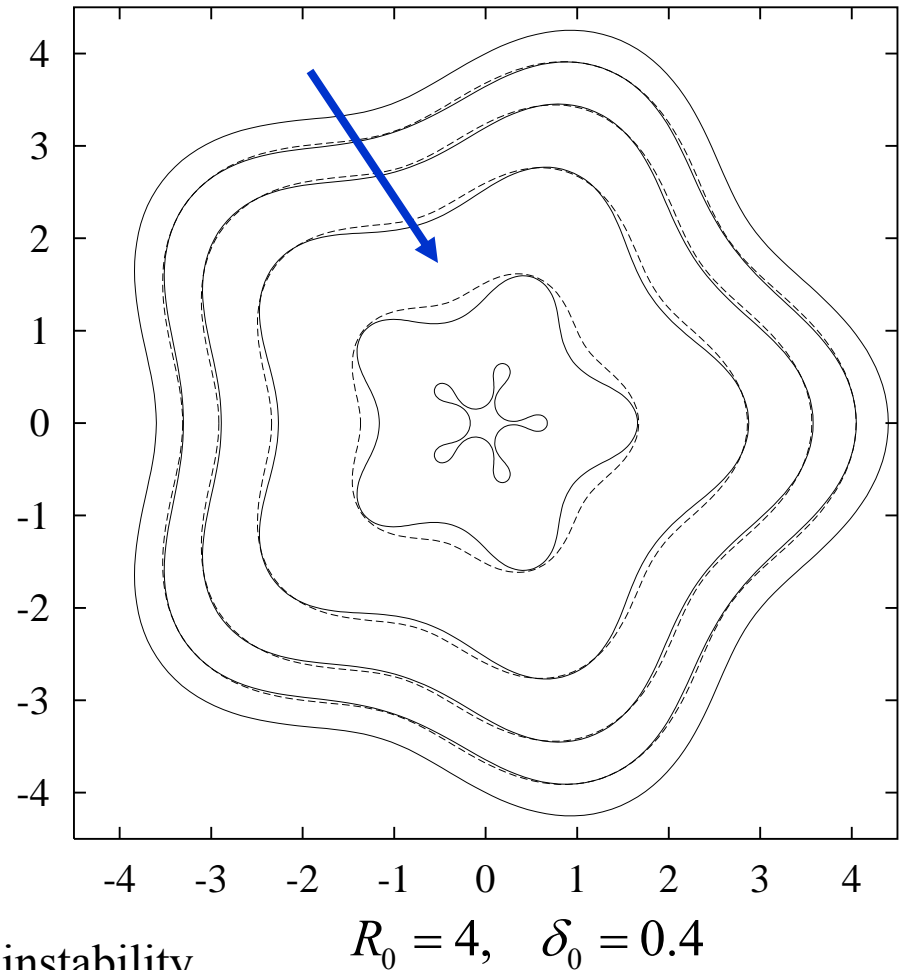
Cristini, Gatenby, et. al., *Clin. Cancer Res.* 11 (2005) 6772.

# Diffusional Instability during shrinkage

$l=5, G=1$

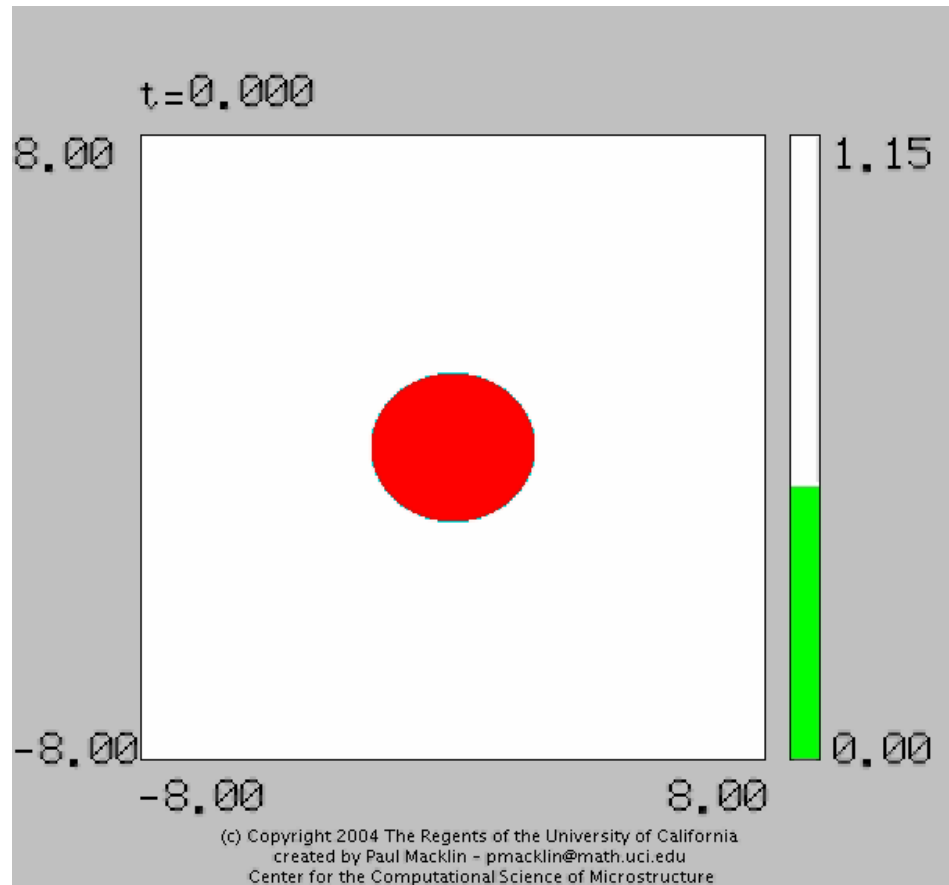
$$A = A^{crit}(l, R, G)$$

- Deviation from linear theory (dashed)
- Fragmentation
- Metastasis
- Implication for therapy
  - Cut off blood supply (antiangiogenic therapy)
  - Radiotherapy/chemotherapy may lead to instability



# Therapy

Vary  $A$  (Radiotherapy)



- Can lead to tumor fission. Metastases.

# Diffusional instability implications

- Fundamental instability
- Increased surface area to volume ratio
- Overcome diffusion-limitations on growth
- Mechanism for invasion of soft tissue
- Topology changes may lead to metastasis
- Therapy may lead to fragmentation and metastasis

## Key features:

- Nonuniform cell-proliferation
- Competition between mitosis, apoptosis and adhesion

# Conclusions

- Basic model is able to capture basic qualitative/quantitative features of tumor growth
- Instability in high vascularization regime requires vascular or mechanical inhomogeneity
- Diffusional instability provides a mechanism to overcome diffusional limitations on growth and can lead to invasive growth and metastasis